Immunotherapy with allergen-loaded nanoparticles containing

lipopolysaccharide from Brucella ovis

Condensed title: Gantrez nanoparticles for immunotherapy

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#### **Abstract**

**Background:** Specific immunotherapy implies certain drawbacks which could be minimized by the use of good adjuvants, capable of amplifying the appropriate immune response with minimal adverse effects.

**Objective:** To evaluate the adjuvant capacity of the association of the rough lipopolysaccharide of *Brucella ovis* with Gantrez<sup>®</sup> AN nanoparticles.

Methods: Ovalbumin (allergen model)-containing Gantrez<sup>®</sup> AN nanoparticles with either encapsulated or coated lipopolysaccharide were prepared and administered intradermally to BALB/c mice in order to evaluate the immune response. Pre-sensitized BALB/c mice were also administered with the formulations and they were challenged with an intraperitoneal injection of ovalbumin. Anaphylactic symptoms, including mortality rates, were evaluated after the challenge.

**Results:** The intradermal administration of mice with ovalbumin-containing nanoparticles elicited high and sustained specific  $IgG_1$  and  $IgG_{2a}$  responses. However, the only treatment that totally protected the mice from death after the challenge of induced allergic mice to ovalbumin, required the co-administration of lipopolysaccharide entrapped inside the nanoparticles.

**Conclusion:** Gantrez<sup>®</sup> AN nanoparticles with entrapped rough lipopolysaccharide of *Brucella ovis* protected ovalbumin pre-sensitized BALB/c mice from anaphylactic shock.

Clinical Implications: These results are highly suggestive for the valuable use of Gantrez<sup>®</sup> nanoparticles combined with lipopolysaccharide of *Brucella ovis* in immunotherapy with allergens.

**Key words:** Gantrez<sup>®</sup>; nanoparticles; adjuvant; lipopolysaccharide; ovalbumin; anaphylactic shock; immunotherapy

#### 1. Introduction

Allergen-specific immunotherapy (SIT) involves repeated administrations of the sensitizing allergen, usually by subcutaneous injection or, more recently, by sublingual application. SIT has been shown to be a robust and clinically effective approach[1, 2], improving the quality of life of the treated individuals, through the reduction of symptoms and medication usage[3].

However, historically, variability in safety and clinical efficacy has limited the widespread application of SIT[4]. Many strategies have been proposed in an attempt to solve these drawbacks, including the use of recombinant allergens and allergen derivatives[5], peptides containing aminoacid sequences of allergen T-cell epitopes[6], low molecular weight fractions of allergen extracts[7], mimotopes[8] and DNA vaccines[9].

The mechanisms by which SIT exerts its effects are not completely known. However, it appears that SIT may modify the response from antigen presenting cells (APCs), and hence of T and B cells in order to neutralize the allergen or to induce its tolerogenicity[10].

SIT effects may be enhanced by the use of adjuvants. However, the most common adjuvants used are aluminium hydroxide, calcium phosphate, and tyrosine, which have a good safety record but elicit a poor T cell response, and the antibodies are mostly of T-helper type 2 (Th2)-type, including IgE[11]. Therefore, the search of new adjuvants is of capital interest. In this context, polymeric nanoparticles could play a key role. This kind of particulate vaccine delivery systems have a lot of advantages such as: i) the protection of the encapsulated active product against its enzymatic inactivation, ii) the increase of the stability of the material incorporated during the manufacturing

process, transport and storage of such active product and iii) the improvement of the efficacy of the presentation to the APCs[12-14]. In this context, this improvement of the antigen presentation could also be ameliorated by the incorporation of a PAMP (pathogen-associated molecular pattern) to nanoparticles.

The dendritic cells (DCs) are APCs involved in initiating, directing and controlling both innate and adaptive immune responses [15, 16]. The recognition of the antigens by the DCs is mediated by their toll-like receptors (TLRs) located on their surface. TLRs are able to recognize PAMPs of the invading microorganisms, and some examples of PAMPs are lipopolysaccharide from gram negative bacteria [17], unmethylated bacterial CpG DNA sequences [18] or peptidoglycans from gram positive bacteria among others [19, 20]. For all these reasons the addition of PAMPs to nanoparticles could be a good strategy to induce or promote activation of TLR-mediated signalling pathways in DCs, maturation of DCs and, consecutively, strong activation of antigen-specific T lymphocytes. In this context some PAMPs, such as lipopolysaccharide or lipid A (which is known to be the region of the lipopolysaccharide responsible for its adjuvant capacity [21]) have been incorporated into some vehicles such as microparticles [22, 23] or nanoparticles [24, 25] in order to enhance their adjuvant effect. However, a main drawback when using LPS is its intrinsic toxicity [15].

Therefore, in this investigation it was selected a rough lipopolysaccharide from  $Brucella\ ovis$ , which is known to be low-endotoxic [16].  $Brucella\ possesses$  an unconventional non-endotoxic lipopolysaccharide that confers resistance to antimicrobial attacks and modulates the host immune response. In this context,  $Brucella\ LPS$ , as a PAMP, promote production of IL-2 and IFN- $\gamma$ , but not IL-4, assisting as a

potential carrier for vaccine development in situations requiring a strong Th1-like response for protection against even xeno-infections [17-21].

Hence, Gantrez<sup>®</sup> nanoparticles containing OVA, as model allergen, and LPS of *Brucella ovis* were prepared. The effect of LPS location (coating the surface or encapsulated into the matrix) in the carriers was evaluated in immunization studies as well as in sensitization experiments and further challenge against OVA.

# 2. Methods

#### 2.1. Chemicals

Gantrez® AN 119 [poly(methyl vinyl ether-co-maleic anhydride); MW 200,000] was kindly gifted by ISP (Barcelona, Spain). Ovalbumin (OVA) (grade V), 1.3-diaminopropane (DP), 2,2′-Azino-bis(3-ethylbenzo-thiazoline-6-sulfonic acid) diammonium salt (ABTS) and alum were purchased from Sigma-Aldrich Chemie (Germany). The peroxidase immunoconjugates (GAM/IgG<sub>1</sub>/PO and GAM/IgG<sub>2a</sub>/PO) were obtained from Nordic Immunology (The Netherlands). The IL-10 ELISA kit was purchased from Biosource International (California, USA). All other chemicals used were of reagent grade and obtained from Merck (Spain).

## 2.2. Rough lipopolysaccharide (LPS) of Brucella ovis extraction

To prepare cells for extraction, tryptic soy broth (TSB) flask were inoculated with fresh cultures of *Brucella ovis* REO 198 strain, and incubated at 37°C for 3 days in air, under constant shaking. The rough lipopolysaccharide fraction was obtained from complete cells as described previously by the phenol-chloroform-petroleum ether extraction method [22, 23].

## 2.3. Preparation of nanoparticles

Gantrez<sup>®</sup> nanoparticles were prepared by a solvent displacement method previously described[24].

# 2.3.1. Preparation of OVA-entrapped nanoparticles (OVA<sup>in</sup>-NP)

OVA<sup>in</sup>-NP was prepared as described elsewhere[25]. Briefly, 5 mg OVA were dispersed in 1 mL acetone by ultrasonication (Microson<sup>TM</sup>) for 1 min under cooling. The OVA dispersion was then added to 4 mL acetone containing 100 mg Gantrez<sup>®</sup> and the mixture was stirred for 30 min at room temperature. Then, the polymer was desolvated by the addition of 20 mL ethanol: water phase (1:1 by volume). The organic solvents were eliminated under reduced pressure (Büchi R-144, Switzerland) and the resulting nanoparticles dispersed in the aqueous media were cross-linked by incubation with 5 μg DP/mg copolymer for 5 min under magnetic stirring at room temperature. Nanoparticles were purified by centrifugation and lyophilised using sucrose 5% as crioprotector.

# $2.3.2.\ Preparation\ of\ LPS-coated/OVA-entrapped\ nanoparticles\ (OVA^{in}\text{-}LPS^{out}\text{-}NP)$

5 mg OVA were dispersed in 1 mL acetone by ultrasonication (Microson<sup>™</sup>) for 1 min under cooling. The OVA dispersion was then added to 4 mL acetone containing 100 mg Gantrez<sup>®</sup> and the mixture was stirred for 30 min at room temperature. Then, the polymer was desolvated by the addition of 20 mL ethanol: water phase (1:1 by volume). The organic solvents were eliminated under reduced pressure (Büchi R-144, Switzerland). The prepared nanoparticles were then incubated with 1 mg LPS in 1 mL of water for 1 h at room temperature under magnetic stirring. Nanoparticles were purified by centrifugation and lyophilised as described above.

# 2.3.3. Preparation of OVA and LPS-entrapped in nanoparticles (OVA<sup>in</sup>-LPS<sup>in</sup>-NP)

5 mg OVA were dispersed in 1 mL acetone by ultrasonication (Microson<sup>TM</sup>) for 1 min under cooling, similarly, 1 mg LPS was also dispersed in 1 mL acetone by ultrasonication (Microson<sup>TM</sup>) for 1 min under cooling. The OVA and the LPS dispersions were added to 3 mL acetone containing 100 mg Gantrez<sup>®</sup> and stirred for 30 min at room temperature. Then, the desolvation of the polymer was induced by the addition of 20 mL ethanol: water phase (1:1 by volume). The organic solvents were eliminated under reduced pressure (Büchi R-144, Switzerland). The resulting nanoparticles dispersed in the aqueous media were cross-linked by incubation with 5 μg DP/mg copolymer for 5 min under magnetic stirring at room temperature. The formulation was purified by centrifugation and lyophilised as described above.

# 2.4. Characterisation of nanoparticles

The particle size and the zeta potential of nanoparticles were determined by photon correlation spectroscopy and electrophoretic laser doppler anemometry, respectively, using a Zetamaster analyser system (Malvern Instruments, UK). The samples were diluted with deionized water and measured at room temperature with a scattering angle of 90°. All measurements were performed in triplicate.

The morphological characteristics of the nanoparticles were observed by scanning electron microscopy (LEO Electron Microscopy Inc, Thornwood, NY) operating at 3kV with a filament current of about 0.5 mA. Prior to observation, the

nanoparticles were coated with a platinum laker of about 2 nm using a Cressington sputter-coated 208HR with a rotatory-planetary-tilt stage, equipped with a MTM-20 thickness controller.

The quantification of the amount of OVA associated to nanoparticles was determined using HPLC. The analysis was performed in a HPLC model 1050 series LC, Agilent (Waldbornn, Germany) coupled with fluorescence detector. Data were analyzed by Hewlett-Packard computer using the Chem-Station G2171 program. The separation was carried out at 25 °C on a reversed-phase Zorbax GF-25 column (4.6 mm x 250 mm; particles size 4  $\mu$ m) obtained from Agilent Technologies (California, USA). The mobile phase composition was phosphate buffer (130 mM NaOH, 20mM KCl, 50mM Na<sub>2</sub>HPO<sub>4</sub>) pH 7, methanol and water (40/10/50 v/v/v). The flow rate was set to 1 ml/min and effluent was monitored with fluorescence detection ( $\lambda_{exc}$ =280 nm  $\lambda_{em}$ =340 nm).

For HPLC analysis, nanoparticles were previously digested with NaOH 0.1N for 24 h at 4°C. Then, the samples were transferred to auto-sampler vials, capped and placed in the HPLC auto-sampler.

The amount of associated LPS to nanoparticles was indirectly estimated by determining one of its exclusive markers, 2-keto-3-deoxy-octulosonic acid (KDO), by the thiobarbiturate acid method[26]. For this purpose, a solution containing digested nanoparticles (NaOH 0.1N, 24h, 4°C) was added to 5 volumes of a solution of methanol and 1% methanol saturated with sodium acetate to precipitate the LPS content. The pellet obtained was then resuspended in 0.2% SDS solution and used in the KDO assay. Each sample was assayed in triplicate and results were expressed as the amount of LPS (in µg) per mg nanoparticles.

#### 2.5. Immunization studies

Animal protocols were performed in compliance with the regulations of the Ethical Committee of the University of Navarra in line with the European legislation on animal experiments (86/609/EU).

BALB/c mice, females of 8 weeks old (supplied by Harlan Interfauna Ibérica, Spain), were randomized into 6 groups of 5 mice. Animals were intradermally immunised once on day 0, with 10 μg OVA incorporated in one of the following formulations: i) OVA-entrapped nanoparticles (OVA<sup>in</sup>-NP); ii) OVA-entrapped and LPS-coated nanoparticles (OVA<sup>in</sup>-LPS<sup>out</sup>-NP); iii) OVA and LPS-entrapped nanoparticles (OVA<sup>in</sup>-LPS<sup>in</sup>-NP); iv) OVA adsorbed in alhydrogel (OVA-Alum) and v) free OVA dissolved in sterile PBS.

Blood samples from the the retroorbital plexus were collected on days 0, 7<sup>th</sup>, 14<sup>th</sup>, 28<sup>th</sup>, 35<sup>th</sup>, 42<sup>nd</sup> and 49<sup>th</sup> post-immunization. The samples were centrifuged (3000 x g, 10 min) and the resulting sera were pooled. Finally, each pool was diluted 1:10 in PBS and stored at -80°C until analysis.

## 2.6. Quantification of anti-OVA antibodies in serum

Specific antibodies against OVA (Ig $G_1$  and Ig $G_{2a}$ ) were determined in the pooled sera by indirect ELISA. Briefly, microtiter wells (cliniplatte EB, Labsystems, Finland) were coated with OVA (1  $\mu$ g/well) at 4°C overnight. Serum samples were added in two-fold serial dilutions in PBS-Tween 20 (1%) starting with 1:40, and

incubated at 37 °C for 4 h. Anti-mouse  $IgG_1$  or  $IgG_{2a}$  peroxidase conjugates diluted 1:1000 in PBS-Tween 20 (1%) were added followed by the substrate chromogen solution ( $H_2O_2$ -ABTS). Optical density (OD) was determined at  $\lambda_{max}$  405 nm (iEMS Reader MF de Labsystems, Finlandia). Measurements were performed by triplicate and data were expressed as the reciprocal of a serum dilution whose optical density was 0.2 above blank samples.

# 2.7. Quantification of IL-10

The IL-10 in the pooled sera of immunized mice was quantified by a commercial ELISA kit of Biosource International (California, USA). Measurements were performed by triplicate and data were expressed as pg/mL of IL-10 in sera.

#### 2.8. Sensitization, vaccination and challenge studies

The scheme of the experiment is shown in Figure 1. Briefly, BALB/c mice, females of 8 weeks old (supplied by Harlan Interfauna Ibérica, Spain), were sensitized by intraperitoneal injection of 50 µg of OVA emulsified in 1 mg alum (alhydrogel) adjuvant (Sigma-Aldrich Chemie, Germany) in a total volume of 150 µL on days 1<sup>st</sup> and 8<sup>th</sup>. On days 14<sup>th</sup>, 17<sup>th</sup> and 20<sup>th</sup>, the animals (5 mice per group) received intradermal injections with 3 µg of OVA each incorporated in either OVA<sup>in</sup>-NP, OVA<sup>in</sup>-LPS<sup>out</sup>-NP or OVA<sup>in</sup>-LPS<sup>in</sup>-NP. As controls, OVA dispersed in Alum (Ova-Alum) and PBS were used. Finally on day 35<sup>th</sup> the animals were challenged by an injection of 1 mg of OVA by intraperitoneal route.

Blood samples from the the retroorbital plexus were collected on days 0, 13<sup>th</sup>, 27<sup>th</sup> and 33<sup>th</sup>. The samples were centrifuged (3000 x g, 10 min) and the resulting sera were pooled. Finally, each pool was diluted 1:10 in PBS and stored at -80°C until analysis.

## 2.8.1. Determination of total immunoglobulin E antibody levels in serum

To determine the IgE antibody level, microtitre plates (Nunc-ImmunoTM Plate, Roskilde, Denmark) were coated overnight at 4°C with anti-mouse IgE antibodies (pH 9.5) (BD OptEIATM Set Mouse IgE, BD Biosciences, Franklin Lakes, NJ, USA). Thereafter, plates were washed with PBS-Tween 20 0.05% (PBS-T20) and blocked for 1 h at room temperature with PBS-FBS 10%, washed again and sera dilutions were incubated for 2 h at room temperature. After washing, plates were incubated for 1 h at room temperature with a mixture of anti-IgE antibodies marked with biotin and horseradish peroxidase-conjugated. Later, plates were washed under the same conditions and 2,20-azino-bis(3-ethylbenzothiazoline-6-sulphonic acid) in citric acid (pH 4.0) and hydrogen peroxide was added. The optical density was measured at 405 nm in a microplate autoreader (iEMS Reader MF, Labsystems).

#### 2.8.2. Histamine quantification

Histamine release test was performed on heparinized whole blood from the retro-orbital plexus obtained before and 30 min after the challenge. Samples were lysed using perchloric acid (1.4% w/w) to determine whole blood histamine content. The resulting suspensions were centrifuged (10 min, 800 x g) and histamine production was

assayed by a fluorometric method as previously described[27] using a Technicon II Analyzer (Technicon Instrument Corp., USA).

## 2.8.3. Evaluation of anaphylaxis

The body temperature changes associated with anaphylactic shock were monitored by measuring the rectal temperature[28] without general anesthesia before and 10 min after the challenge. Anaphylactic symptoms (activity, bristly hair, and cyanosis) were evaluated 30 min after the challenge using a scoring system modified from previous reports[29, 30]. Reactions severity was classified in following categories depending on their gravity: i) (-) absent; ii) (+) weak; iii) (++) moderate; and iv) (+++) strong, and the mobility was classified in i) low or ii) normal, depending on the activity of the animals. Finally, the mortality rates were recorded 24 h after intraperitoneal challenge.

## 2.9. Statistical analysis

The physico-chemical characteristics were compared using the Student t-Test. P values <0.05 were considered significant. For the evaluation of the histamine increase and temperature decrease, statistical comparisons were performed using the one-way analysis of variance test (ANOVA) and Tukey HSD test. P<0.05 was considered as a statistically significant difference. All calculations were performed using SPSS® statistical software program (SPSS® 10, Microsoft, USA).

#### 3. Results

# 3.1. Characterisation of Gantrez® nanoparticles

The main physico-chemical characteristics of Gantrez<sup>®</sup> formulations are summarised in Table 1. The size of OVA nanoparticles were significantly higher than empty nanoparticles (NP) (p<0.05); however, the presence of LPS in the OVA formulations did not affect the size of the nanoparticles. Overall, nanoparticle batches were found to be homogeneous spheres (Figure 2). In addition, no important difference was visualized when compared SEM photographs of nanoparticles containing only OVA (OVA<sup>in</sup>-NP, Figure 2a) with nanoparticles containing also LPS (OVA<sup>in</sup>-LPS<sup>in</sup>-NP, Figure 2b). The OVA content was about 25-30 μg/mg in all cases and the LPS amount was around 14 μg/mg nanoparticles.

Concerning the OVA content, it is interesting to note that the addition of LPS slightly decreased the OVA content and the encapsulation efficiency.

3.2. Antibody response in BALB/c mice after intradermal administration of the OVA-nanoparticle formulations

Figure 3 shows the anti-OVA  $IgG_1$  and  $IgG_{2a}$  titres (Th2 and Th1 markers, respectively) in sera after intradermal immunization of mice with the different formulations. All nanoparticle formulations induced a similar profile characterised by a short lag-time, of about 1 week, followed by a rapid increase of anti-OVA  $IgG_1$  levels for at least 3 weeks. At the end of this period (day  $28^{th}$ ), a plateau of antibody levels was reached and maintained till the end of the experiment (day  $49^{th}$ ). The levels of anti-OVA

 $IgG_1$  antibodies were always higher for nanoparticle formulations than those induced by the control OVA-Alum. On the other hand, the presence of LPS on the surface of the nanoparticles (OVA<sup>in</sup>-LPS<sup>out</sup>-NP) increased the level of  $IgG_{2a}$  antibodies against OVA (Th1 response). Free OVA titres were close to the basal line.

# 3.3 IL-10 quantification

Figure 4 shows the IL-10 concentration in sera after intradermal immunization of mice with the different nanoparticles formulations. OVA<sup>in</sup>-NP appeared to be the most effective formulation in inducing IL-10 production. On the other hand, the association of LPS to the nanoparticles decreased the seric levels of IL-10. Significantly, a peak of IL-10 concentration was found on day 14<sup>th</sup> for all OVA-entrapped nanoparticles,

#### 3.4. Immunotherapeutic schedule

The induced OVA-allergic mice received the immunotherapeutic schedule previously described, and IgE levels were monitorised on days 0, 13, 27 and 33. These levels were found to be higher for the animals immunized with OVA-Alum than those with OVA<sup>in</sup>-LPS<sup>out</sup>-NP and OVA<sup>in</sup>-LPS<sup>in</sup>-NP (Figure 5) during all the experiment. Furthermore, at day 35, the amount of IgE for the OVA-Alum group was two times higher than the one produced by mice immunized with every OVA nanoparticles formulations (OVA <sup>in</sup>-NP, OVA <sup>in</sup>-LPS <sup>out</sup>-NP and OVA <sup>in</sup>-LPS <sup>in</sup>-NP).

On day 35<sup>th</sup> the animals were challenged with OVA. In order to analyse the intensity of the anaphylactic shock, several parameters were determined. Figure 6 shows the difference of histamine blood levels before the challenge and 30 minutes later. Groups treated with either OVA<sup>in</sup>-LPS<sup>in</sup>-NP or OVA<sup>in</sup>-NP showed a significant lower increase of the histamine levels in comparison with the control groups (OVA-Alum and PBS). In contrast, the group of animals treated with OVA<sup>in</sup>-LPS<sup>out</sup>-NP did not show a significant difference with the controls.

Table 2 shows the overall anaphylactic symptoms score including the mortality rate. OVA<sup>in</sup>-NP, OVA<sup>in</sup>-LPS<sup>out</sup>-NP and OVA<sup>in</sup>-LPS<sup>in</sup>-NP groups showed a slightly lower decrease on the body temperature than the controls (OVA-Alum and PBS), although, the differences were not significant (p<0.05). The piloerection and cyanosis seemed to be lower for OVA<sup>in</sup>-NP and OVA<sup>in</sup>-LPS<sup>in</sup>-NP than for the other formulations. Furthermore, the mobility seemed not to be affected in the animals treated with OVA<sup>in</sup>-LPS<sup>in</sup>-NP, while for the other groups the animals were found to be static with a high difficulty to coordinate any simple movement. Finally, the OVA<sup>in</sup>-LPS<sup>in</sup>-NP group protected the animals from death, while, for the other groups tested, the mortality rate was between 40 and 80%.

#### 4. Discussion

The physicochemical and biodegradation properties of some nanoparticle formulations may be worthy as useful imunoadjuvants[31-33]. In the context of the immunotherapy of allergic processes, potent adjuvants are required. Thus, and based on previous studies with nanoparticles of the polymer Gantrez<sup>®</sup> AN[25], the aim of the present work was to study the effect of the incorporation of an immunostimulant, such as the low-endotoxic LPS from *Brucella ovis*[34], on the adjuvant capacity of these nanoparticles. The special chemical nature of Gantrez<sup>®</sup> nanoparticles may afford the binding on their exposed chemical reactive groups of microbial markers, that may interact with scavenger ligands on the immune cells involved in signal transduction and the secretion of cytokines[34]. For this purpose, Gantrez<sup>®</sup> nanoparticles containing ovalbumin (OVA) were prepared. This protein was incorporated during the manufacture process (OVA-entrapped nanoparticles) as described previously[25], and the LPS was incorporated either during the nanoparticle manufacture (LPS<sup>in</sup>, entrapped) or after the preparation of nanoparticles (LPS<sup>out</sup>, coating).

When these formulations were intradermally administered to mice, the presence of the LPS on the NP (OVA<sup>in</sup>-LPS<sup>out</sup>-NP) increased the OVA-specific IgG<sub>2a</sub> levels (Th1 marker). On the contrary, the levels of IgG<sub>1</sub> (Th2 marker) were not affected by the presence of the LPS. These results are in agreement with our previous observations related with the ability of *Brucella ovis* LPS to promote the production of Th1 cytokines[35]. Thus, OVA<sup>in</sup>-LPS<sup>out</sup>-NP (LPS coating the surface of nanoparticles) is "mimicking" the gram negative bacteria structure with the LPS on the surface, activating the Th1 pathway. Other authors have used smooth *Brucella spp*. lipopolysaccharides in assisting as a potential carrier for vaccine development in

situations requiring a strong Th1-like response for protection against even xeno-infections[17, 19-21, 36], but this is the first report describing the capability of *Brucella ovis* rough LPS as an immunostimulant.

From the immunological point of view, an allergic episode is characterized by the presence of IgE and IgG<sub>1</sub>, produced by B lymphocytes after the polarization of Th naïve lymphocyte into a Th2 subset population[37]. As it is well known, immunotherapy in humans should be based on the decrease of the Th2 by enhancing the Th1, and this balance is achieved by increasing the activity of the  $T_{reg}$  lymphocytes[38].  $T_{reg}$  cytokines (IL-10, TNF- $\alpha$ ) play a key role in preventing IgE and Th2 expansion[39, 40]. Thus, we have demonstrated that LPS-nanoparticles do exert an effect on the  $T_{reg}$  lymphocites, since IL-10 could be detected after immunization. Moreover, only when OVA was associated to Gantrez<sup>®</sup> nanoparticles, IL-10 could be detected in sera (see Figure 4).

In order to evaluate the therapeutic effect of these formulations with or without LPS on a model of OVA-sensitized mice, the mice were treated with the OVA-entrapped nanoparticles with or without LPS by intradermal route and finally were challenged and the different anaphylactic symptoms were observed. The monistorisation of the total IgE during the experiment indicated that all the formulations of OVA-Gantrez nanoparticles were able to decrease this antibody isotype, which is related to the allergic episodes. Moreover, the formulations with LPS of *Brucella ovis*, showed levels of total IgE even lower than the OVA-NP formulation.

On the other hand, histamine levels, one the most dangerous substance released during anaphylaxis, was much lower (p<0.005) for LPS-entrapped nanoparticles (OVA<sup>in</sup>-LPS<sup>in</sup>-NP) than for control groups (Figure 6). These results correlated well with

the temperature decrease after the challenge (Table 2). However, the ultimate parameter to test the efficacy of the immunization was the protection against mortality. Again, OVA<sup>in</sup>-LPS<sup>in</sup>-NP was found to be the best formulation. In fact, OVA<sup>in</sup>-LPS<sup>in</sup>-NP protected all the mice from death, in contrast to the control groups immunized with OVA-Alum or PBS. However, when the LPS was coating the nanoparticles (OVA<sup>in</sup>-LPS<sup>out</sup>-NP), the mice were not protected, and the mortality rate was similar than that observed for the untreated group. The appropriate co-stimulation of the dendritic TLR-4 with the LPS at the time of allergen (OVA) exposure would develop a protective Th1 immune response. When the LPS is encapsulated in the nanoparticles with the OVA (OVA<sup>in</sup>-LPS<sup>in</sup>-NP), both LPS and OVA are supposed to release at the same time, being more effective the OVA presentation. However, when the OVA is entrapped in the nanoparticles and the LPS is coating the surface (OVA<sup>in</sup>-LPS<sup>out</sup>-NP), the LPS would be released first followed by the OVA.

We have demonstrated the ability of Gantrez<sup>®</sup> nanoparticles to induce high levels of IL-10 thus showing highly interesting adjuvant properties for immunotherapy. However, the most remarkable finding is the capability of combined use of the innocuous rough LPS from *Brucella ovis* and Gantrez<sup>®</sup> nanoparticles to protect from anaphylactic shock. And, it is even more interesting when considering that protection from anaphylactic death is not usually described in the literature [41-44]. Therefore, this effect is a significant finding for its application in immunotherapy.

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# Figure legends

**Figure 1.** Experimental design. BALB/c mice were sensitized by receiving two intraperitoneal injections of 50 μg OVA/Alum. Once the animals were sensitized to OVA, they received the treatments (A) OVA-Alum, PBS, OVA<sup>in</sup>-NP, OVA<sup>in</sup>-LPS<sup>out</sup>-NP and OVA<sup>in</sup>-LPS<sup>in</sup>-NP. Finally, on day 35<sup>th</sup> they were challenged by administering an intraperitoneal injection of 1 mg OVA in solution.

**Figure 2.** SEM photographs of: a) **OVA**<sup>in</sup>**-NP** (OVA-entrapped nanoparticles) and b) **OVA**<sup>in</sup>**-LPS**<sup>in</sup>**-NP** (OVA and LPS-entrapped nanoparticles).

**Figure 3**. Anti-OVA IgG<sub>1</sub> and IgG<sub>2a</sub> titres in sera after intradermal immunization with: OVA solution (OVA) ( $\blacksquare$ ), OVA adsorbed in alhydrogel (OVA-Alum) ( $^{\bigstar}$ ), OVA-entrapped nanoparticles (OVA<sup>in</sup>-NP) ( $\triangle$ ), OVA-entrapped and LPS-coated nanoparticles (OVA<sup>in</sup>-LPS<sup>out</sup>-NP) ( $\triangle$ ), and OVA and LPS entrapped nanoparticles (OVA<sup>in</sup>-LPS<sup>in</sup>-NP) ( $^{\nabla}$ )). The antibody titre is defined as the reciprocal dilution giving an optical density (OD) reading at 405 nm of  $\ge$  0.2.

**Figure 4**. IL-10 concentration (pg/mL) in sera after intradermal immunization with OVA solution (OVA) ( $\blacksquare$ ), OVA adsorbed in alhydrogel (OVA-Alum) ( $^{\bigstar}$ ), blank nanoparticles (NP) ( $\spadesuit$ ), OVA-entrapped nanoparticles (OVA<sup>in</sup>-NP) ( $\triangle$ ), OVA-entrapped and LPS-coated nanoparticles (OVA<sup>in</sup>-LPS<sup>out</sup>-NP) ( $\Delta$ ) and OVA and LPS entrapped nanoparticles (OVA<sup>in</sup>-LPS<sup>in</sup>-NP) ( $^{\nabla}$ )).

**Figure 5**. Evolution of total IgE in sera from BALB/c mice during the sensitization and challenge study. Mice were sensitized to OVA (50 μg OVA by an intraperitoneal route, days 1 and 8) and immunized (10 μg OVA, divided in to three doses of 3.33 μg; (see arrows ( $\downarrow$ ) in the figures) with OVA adsorbed in aluminium hydroxide (OVA-Alum) ( $^{\bigstar}$ ) OVA-entrapped nanoparticles (OVA<sup>in</sup>-NP) ( $\Delta$ ), OVA-entrapped and LPS-coated nanoparticles (OVA<sup>in</sup>-LPS<sup>out</sup>-NP) ( $\Delta$ ) and OVA and LPS entrapped nanoparticles (OVA<sup>in</sup>-LPS<sup>in</sup>-NP) ( $\nabla$ )).

**Figure 6**. Increase of the histamine blood level after the challenge with 1 mg of OVA i.p. After sensitization to OVA, the different groups of animals were treated (days 14<sup>th</sup>, 17<sup>th</sup> and 20<sup>th</sup>) with OVA-entrapped nanoparticles (OVA<sup>in</sup>-NP), OVA-entrapped and LPS-coated nanoparticles (OVA<sup>in</sup>-LPS<sup>out</sup>-NP) and OVA and LPS entrapped nanoparticles (OVA<sup>in</sup>-LPS<sup>in</sup>-NP). OVA adsorbed in alhydrogel (OVA-Alum) and PBS were used as controls. (\*) represents statistical difference (p <0.5).

**Table 1.** Physico-chemical characteristics of Gantrez<sup>®</sup> nanoparticles. Data were represented by mean  $\pm$  SD (n=10).

Formulations <sup>(a)</sup>	LPS content (µg/mg)	OVA content (µg/mg)	Encapsulation efficiency (%)	Size (nm)	Zeta Potential (mV)
NP	-	-	-	158±3	-45.1±0.5
OVA <sup>in</sup> -NP	-	30.1±4.5	42.1±6.3	239±4	-50.8±2.9
OVA <sup>in</sup> -LPS <sup>out</sup> -NP	15.2±0.5	24.1±5.4	33.9±7.6	231±3	-46.1±3.1
OVA <sup>in</sup> -LPS <sup>in</sup> -NP	13.8±3.0	26.5±0.3	37.3±0.4	227±4	-34.1±3.4

<sup>(</sup>a) Formulations: **NP**: empty nanoparticles; **OVA**<sup>in</sup>-**LPS**<sup>out</sup>-**NP**: OVA-coated and LPS-entrapped nanoparticles; **OVA**<sup>in</sup>-**NP**: OVA-entrapped nanoparticles; **OVA**<sup>in</sup>-**LPS**<sup>out</sup>-**NP**: OVA-entrapped and LPS-coated nanoparticles; **OVA**<sup>in</sup>-**LPS**<sup>in</sup>-**NP**: OVA and LPS-entrapped nanoparticles.

**Table 2.** Anaphylactic symptoms in the treated vs. non-treated OVA allergic mice.

Immunotherapeutic treatment <sup>(a)</sup>	Temperature decrease (°C)	Piloerection	Mobility	Cyanosis	Mortality rate (%)
OVA-Alum	3.62±1.03	++	Low	++	80
PBS	3.54±3.14	+++	Low	+++	60
OVA <sup>in</sup> -NP	2.96±1.42	+	Low	+	40
OVA <sup>in</sup> -LPS <sup>out</sup> -NP	2.83±1.27	+++	Low	+++	60
OVA <sup>in</sup> -LPS <sup>in</sup> -NP	1.19±1.42	+	Normal	++	0

Severity of the symptoms: (-) absent; (+) weak; (++) moderate and (+++) strong.

(a) Treatments: **OVA-Alum**: OVA adsorbed to aluminium hydroxide; **PBS**: Phosphate buffer saline; **OVA**<sup>in</sup>-**NP**: OVA-entrapped nanoparticles; **OVA**<sup>in</sup>-**LPS**<sup>out</sup>-**NP**: OVA-entrapped and LPS-coated nanoparticles; **OVA**<sup>in</sup>-**LPS**<sup>in</sup>-**NP**: OVA and LPS-entrapped nanoparticles.

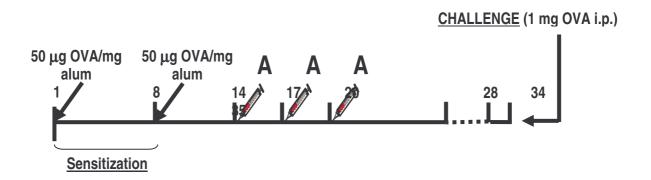


Figure 1

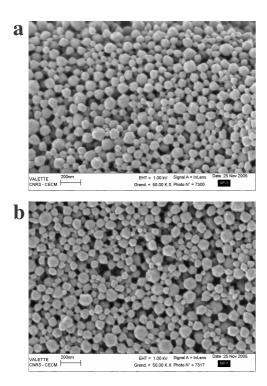


Figure 2

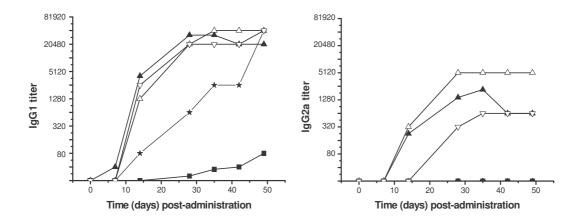


Figure 3

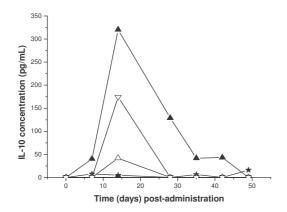


Figure 4

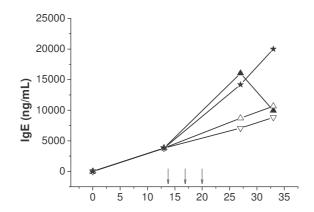


Figure 5

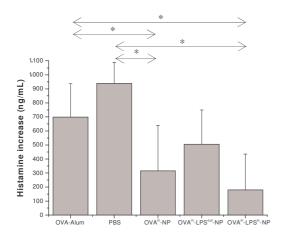


Figure 6